ejpmr, 2018,5(2), 428-436



EUROPEAN JOURNAL OF PHARMACEUTICAL AND MEDICAL RESEARCH

www.ejpmr.com

Research Article ISSN 2394-3211 EJPMR

A STUDY ON PROCESS DRIFT OF DIRECTLY COMPRESSIBLE MATRIX TABLETS OF ISONIAZID

Surendra Agrawal*¹, Pratushti Mittal¹ and Shishupal Bodhankar²

^{1,3}Shobhaben Pratapbhai Patel School of Pharmacy and Technology Management, SVKM'S NMIMS, Mumbai, India 400056.

²Bajiraoji Karanjekar College of Pharmacy, Sakoli, Dist- Bhandara, Maharastra (India) 441802.

*Corresponding Author: Dr. Surendra Agrawal

Shobhaben Prataphai Patel School of Pharmacy and Technology Management, SVKM'S NMIMS, Mumbai, India 400056.

Article Received on 18/12/2017

Article Revised on 07/01/2018

Article Accepted on 28/01/2018

ABSTRACT

Solid oral dosage forms are the preferred route for many drugs and are still the most widely used formulations. Of these, tablets offer the lowest cost approach. Matrix tablets serves as an important tool for oral dosage forms. Pharmaceutical industry engaged in making solid dosage form is facing critical problems in proving their process reproducibility. Even that has reduced profits, especially because of critical deviations which are consequences of continuous process and inadequate research. Up-scaling can be challenging as minor changes in parameters can lead to varying quality results. The main objective of the work was to select critical process parameters (CPP) using retrospective data of a developed product and to establish a design of experiments (DoE) that would improve the robustness of the tableting process. Batches were selected based on the quality results generated during batch release, some of which revealed quality deviations concerning the appearance of the coated tablets. The Minitab 17 software was used for data processing to determine critical process parameters and create design spaces based on retrospective data of production batches. This type of analysis is thus converted into a tool to optimize the robustness of existing processes. This study will help to determine a design space which can be established with minimum investment in experiments.

KEYWORDS: Direct compression, Formulation variables, Process variables, matrix tablets, Isoniazid.

1. INTRODUCTION

A process drift is an unintended, unexplained or unexpected trend of measured process parameter(s) and/or resulting product attribute(s) away from its intended target value in a time- ordered analysis over the lifetime of a process or product. Process drift is the consequence of variation in a variety of process inputs, including raw materials, manufacturing personnel, and machine (man-machine) interactions or processing conditions. When robust systems are not implemented and capable tools are not used to prevent process drift, resulting manufacturing problems may include: low product yield, batch delays, ingredient and packaging variability, batch failures, product quality-related clinical failures, investigations, recalls, product seizures, injunctions, and consent decrees.^[1] The use of tools and approaches such as process analytical technologies (PATs), ObD, in vitro-in vivo correlation (IVIVC), and more thorough excipient characterization should improve the robustness of the finished products and minimize or prevent unintended drift in the quality of the affected commercial drug products.^[2]

Many studies on the influence of the powder's mechanical characteristics on the performance of the tablet have been performed in the past.^[3-14] Optimization technique is an ideal tool for preparing better quality of dosage forms. This technique is widely used for developing optimal dosage forms and a better process of manufacture.^[15]

Optimization was considered as an economical and efficient method which helps understand the relationship between independent and dependent variables. Optimization has been gaining popularity in pharmaceutical research, day by day, since the best results can be obtained in a limited number of experiments.^[16]

Direct compression involves simple blending of active pharmaceutical ingredient (API) with other ingredients and direct compaction of the resultant mixture. In contrast to direct compression, wet granulation not only increases the cycle time, but also has certain limits imposed by thermolability and moisture sensitivity of the active ingredient. The unnecessary exposure of any drug to moisture and heat remains unjustified. Low dilution potential (30%-40% of the drug in the formulation) and the segregation due to the difference in density between API and excipients.^[17]

The use of matrix technology has been a commercial success and the pharmaceutical marketplace witnessed a large number of novel drug delivery systems based on them. Matrix polymers help to opportunely modulate and modify the drug release from modified drug delivery systems.^[18,19] Isoniazid (INH) is known to be one of the most efficacious anti-TB drugs and is recommended by WHO. It possesses many advantages such as high selectivity towards *Mycobacterium tuberculosis*, excellent bacteriostatic capacity, low price and good patient compliance.^[20] Isoniazid here was selected as a model drug in the study.

In pharmaceutical industries, manufacturers of generic tablets are usually focused on the optimization of the excipient mixture composition to obtain a product that meet established standards. Several tablet compositions of extended and fast release have been established using statistical design to optimize excipient proportions. However tablet properties do not only depend on the excipient percentage in the solid dosage. Various process variables like compression and granulation i.e., compaction force, compression velocity, tableting temperature, impeller speed and blending time can also have influences.^[21,22]

2. MATERIALS AND METHODS

2.1 Formulation of Directly compressed matrix tablets of INH

The matrix tablets of INH were made as per the set specification as mentioned in Table 1. All the ingredients were sifted through # 40 sieve and Physical mixing of Isoniazid and PMC K100M was done geometrically. It was combined with dibasic calcium phosphate and Colloidal silicon oxide (Aerosil). Lubricant Magnesium stearate was mixed and powder blend formed. The blend was compressed by direct compression method using D- tooling (12.5 mm punch size). The tablets were scored.^[23,24] Three batches I, II and III of Isoniazid were formulated using matrix tablets varving combinations of the polymer HPMC K100M and Dibasic calcium phosphate as shown in Table 2. The amount of API, Colloidal silicon oxide and magnesium stearate was kept constant.

Three new batches IV, V and VI were formulated keeping the amount of dibasic calcium phosphate constant with 87 mg/ tablet in all three batches as given in Table 2. Variation in the amount of HPMC was made to study the effect of concentration of HPMC polymer on drug release. The concentration of all other excipients was kept constant in all the three batches. Powder blend was analyzed for all the batches prior tablet compression. The Carr's compressibility index and Hausner's ratio was calculated for the powder blend and the evaluation of tablets was performed as per IP 2007.^[25]

2.2 Design of Experiment

The DOE trials were carried out to see the influence of different variables on the formulation development. In this study, Concentration of Dibasic calcium phosphate and Compression force were taken as Independent variables and In-vitro drug release and Content uniformity of tablets were considered as dependent variables. The study was designed using Minitab 17 software.^[1,26] A 3^2 factorial design was used for the application of DOE. Total nine batches were formulated as given in Table 3.

2.3 Release Studies

Dissolution studies were performed in two dissolution media, 0.1 N hydrochloric acid followed by Phosphate buffer pH 6.8 using Basket type USP Dissolution apparatus at 50 RPM. Dissolution in acidic media was for 2 hrs subsequently for 1 hr by replacing dissolution media with buffer. Five ml aliquot was withdrawn and replaced with fresh media each time. UV readings were taken at 263 nm (λ max of Isoniazid) and concentrations of Isoniazid were calculated in each aliquot. In-vitro drug release study performed for 24 hours.^[27,28]

3. RESULTS AND DISCUSSION

3.1 Evaluation of Powder blend and Isoniazid matrix tablets

All batches were first analyzed for powder flow properties as per USP 2016 (NF 37) and tablet evaluation as per IP 2014. Evaluation of powder blend is necessary to understand its flow properties and compressibility which will play a vital role during tablet compression.^[29]

Comparison of the obtained values of Carr's index and Hausner's ratio for batches I, II and III to that specified in USP 2016 (NF 37) showed that all three batches had very poor to fair flow properties.^[28] Batches IV, V and VI revealed fair flow as shown in the Table 4. All tablets were white in color, showed no chipping or cracking and resulted in good aesthetic appeal with defined content uniformity range and acceptable weight uniformity. Invitro drug release study was performed on all batches, however batch II showed a consistent drug release for 26 hours and zero burst release as shown in Fig 1. Thus, batch II was chosen for further optimization using DoE trials.

3.2 DOE trials

All batches for DOE trials were evaluated for their powder flow properties before tablet compression. Further tablet evaluation was performed on all the batches and the results are mentioned in Table 5 and 6.

Tablets obtained from all batches had good aesthetic appeal with desired hardness levels. Even though the values of % friability decreased with an increase in

hardness from 7 to 11, all batches passed the friability test. From the above table it can be seen that all the batches confirmed with the uniformity of weight test and had acceptable content uniformity.

Batch VII, VIII and IX showed less than 45% drug release in the first 2 hours. This is attributed to the low amount (69.6 mg/tablet) of DCP in the formulation.

Batch X with DCP concentration 87 mg/tablet showed 48% drug release in first 2 hours followed by 99% at the end on 24 hours. The hardness of batch X was 7 kg/cm2. In contrast to this, batches XI and XII released a total of 89% and 87% of API.

As depicted in fig 3, only batches XIII, XIV and XV showed 50 % and more drug release as a consequence of difference in compression force varying from 7, 8 and 9 kg/cm2 respectively with a constant amount of Dibasic calcium phosphate. Increase in tablet hardness resulted in slower drug release from the formulation thus prolonging the duration of release.

Pareto charts as shown in Fig 4 (A & B) revealed that the concentration of dibasic calcium phosphate does not significantly affected both drug release and % friability. Whereas, compression force applied during tablet manufacturing significantly affected the drug release and % friability. There was not much impact of amount of DCP and compression force on drug release and % friability but the amount of DCP had a significant impact on the Content uniformity of the tablets as revealed in Fig 4 (C). Compression force had less significant impact on content uniformity of the tablets. A combination of DCP concentration and compression force had the least role to play in content uniformity of the tablets.

Contour plots display the 3-dimensional relationship in two dimensions, with x- and y- factors (predictors) plotted on the x- and y-scales and response values represented by contours. A contour plot is like a topographical map in which x-, y-, and z-values are plotted instead of longitude, latitude, and elevation. Fig 5 (A) revealed that design space to obtain a 100% drug release for dibasic calcium phosphate was found between 90 to 105 mg/tablet. Design space for Compression force was between 7 to 7.4 kg/cm2. As shown in Fig 5 (B), design space to obtain % friability in permissible limits for dibasic calcium phosphate was found between 90 to 105 mg/tablet. Design space for compression force was between 10 to 11 kg/cm2. As shown in Figure 5 (C), design space to obtain content uniformity in permissible limits for dibasic calcium phosphate was found between 73 to 84 mg/tablet. Design space for Compression force was between 7.2 to 7.5 kg/cm2.

In the present study, HPMC concentration was kept constant considering its suitability with dibasic calcium phosphate in making directly compressible matrix tablets. Dibasic calcium phosphate concentration and compression has significant effect on the friability and release property of the matrix tablets. Design of experiment helped in designing and optimization process and also to understand the process drift. The Critical limits developed through these kind of studies would lead to a robust process for manufacturing directly compressible matrix tablets.^[30,31]

C	ations of	INH matrix tablets.	
	S. No:	Elements of INH Tablet	Target
	1	Dosage form	Tablet
	2	Dosage design	Sustained release matrix tablet
	3	Route of administration	Oral
	4	Dosage strength	300 mg
	5	Therapeutic moiety/ delivery	Swelling, gelling and drug release
	6	Appearance	White, scored
	7	Weight of the tablet	Average weight \pm 5%
	8	Diameter of the tablet	$12.5 \text{ mm} \pm 0.12 \text{ mm}$
	9	Dissolution time	24 hours

Table No 1: Specifications of INH matrix tablets.

Table N	lo 2:	Formulation	trials of	INH	tablets	(Batches I to V	I).

	Quantity (mg/tablet) used per batch									
Batch I Batch II Batch III Batch IV Batch V										
Ingredients	100	100	100							
Batch size	tablets	tablets	tablets							
Isoniazid (B.No:14344/INH)	300	300	300	300	300	300				
HPMC K100M	200	250	300	200	250	300				
Dibasic calcium phosphate	137	87	37	87	87	87				
Colloidal silicon oxide	6.5	6.5	6.5	6.5	6.5	6.5				
Magnesium stearate	6.5	6.5	6.5	6.5	6.5	6.5				
Total weight (mg/ tab)	650	650	650	600	650	700				

Table No 3: Formulation of DO	E trials Batch VII to Batch XV.

		Quantity (mg/tablet) used per batch								
	B-VII	B-VIII	B-IX	B- X	B-XI	B- XII	B-XIII	B-XIV	B- XV	
Ingredients										
Batch size (No. of tablets)	150	150	150	150	150	150	150	150	150	
Isoniazid (B.No:14344/INH)	300	300	300	300	300	300	300	300	300	
HPMC K100M	300	300	300	300	300	300	300	300	300	
Dibasic calcium phosphate	69.6	69.6	69.6	87	87	87	104.4	104.4	104.4	
Colloidal silicon oxide	6.5	6.5	6.5	6.5	6.5	6.5	6.5	6.5	6.5	
Magnesium stearate	6.5	6.5	6.5	6.5	6.5	6.5	6.5	6.5	6.5	
Total weight (mg/ tab)	682.6	682.6	682.6	700	700	700	717.4	717.4	717.4	
Compressionforce(kg/cm2)	7	9	11	7	9	11	7	9	11	

Table 4: Flow properties of powder blend of INH tablets (Batches I to VI).

	Parameters									
Batch No:	Bulk density (Db)	Tapped density (Dt)	Carr's index [(Dt- Db)/ Dt] *100	Flow character	Hausner's ratio (Dt/Db)	Flow character				
Batch I	0.43	0.640	32.81%	Very poor flow	1.48	Very poor flow				
Batch II	0.451	0.549	17.85%	Fair flow	1.21	Fair flow				
Batch III	0.453	0.567	20.10%	Fair flow	1.25	Fair flow				
Batch IV	0.392	0.491	20.16%	Fair flow	1.252	Fair flow				
Batch V	0.405	0.499	18.83%	Fair flow	1.23	Fair flow				
Batch VI	0.405	0.499	18.83%	Fair flow	1.23	Fair flow				

S. N.	Parameters		Batch No								
		Batch I	Batch II	Batch III	Batch IV	Batch V	Batch VI				
1	Divisional appropriation	White, smooth, no	White, smooth, no	White, smooth, no	White, smooth,	White, smooth, no	White, smooth, no				
1	Physical appearance	cracks seen	cracks seen	cracks seen	no cracks seen	cracks seen	cracks seen				
2	Hardness (kg/cm ²)	6	7	6.5	8	7.5	7.5				
3	Average diameter	12.59	12.58	12.59	12.56	12.57	12.57				
4	Average Thickness	4.33	4.65	4.72	3.85 mm	4.67 mm	4.87 mm				
5	Uniformity of weight	650 ±10 mg	650 ±10 mg	$650 \pm 10 \text{ mg}$	$600 \pm 20 \text{ mg}$	$650 \pm 15 \text{ mg}$	$700 \pm 15 \text{ mg}$				
6	% Friability	0.5%	0.48%	0.77%	0.49%	0.69%	0.48%				
7	Content uniformity	99-101%	98-100 %	98.5-100.5 %	98-100 %	99-101 %	98.5-100.5%				

Table 5: Characterization of INH matrix tablets (Batches I to VI).

Table 6: Characterization of INH matrix tablets (Batches VII - XV).

S. N.	Parameters		Batches								
		B-VII	B-VIII	B-IX	B- X	B-XI	B- XII	B-XIII	B-XIV	B- XV	
1	Physical appearance	White	White	White	White	White	White	White	White	White	
2	Hardness (kg/cm ²)	7	9	11	7	9	11	7	9	11	
3	Average diameter	12.60	12.6	12.58	12.57	12.57	12.56	12.60	12.63	12.61	
4	Average thickness	4.96	4.83	4.73	4.88	4.66	4.61	5.32	5.17	4.95	
5	Uniformity of weight	682.6 ± 20	682.6 ± 15	682.6 ± 20	700 ± 10	700 ± 12	700 ± 20	717.4 ± 15	717.4 ± 18	717.4 ± 20	
6	% Friability	0.71%	0.62%	0.48%	0.69%	0.53%	0.42%	0.66%	0.51%	0.30%	
7	Content uniformity	99-101%	98-100%	99.2-100%	98-101%	98-100%	98.2-100%	98-99.8%	99-100%	98-100%	

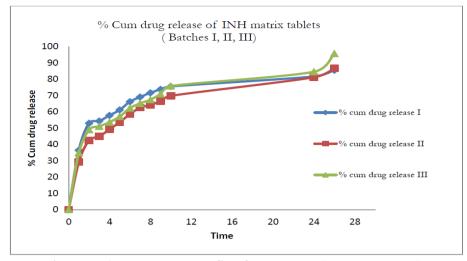


Figure No 1: Drug release profile of INH tablets (Batches I, II, III).

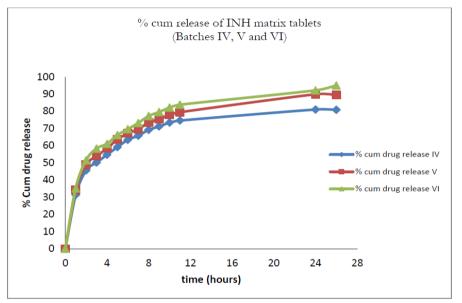


Figure No 2: Drug release profile of INH tablets (Batches IV, V, VI).

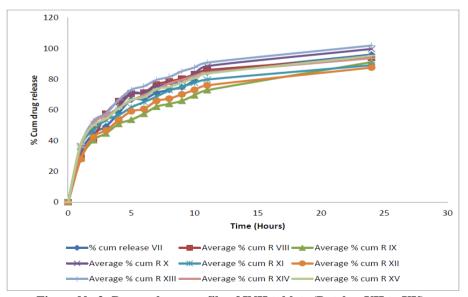


Figure No 3: Drug release profile of INH tablets (Batches VII to XV).

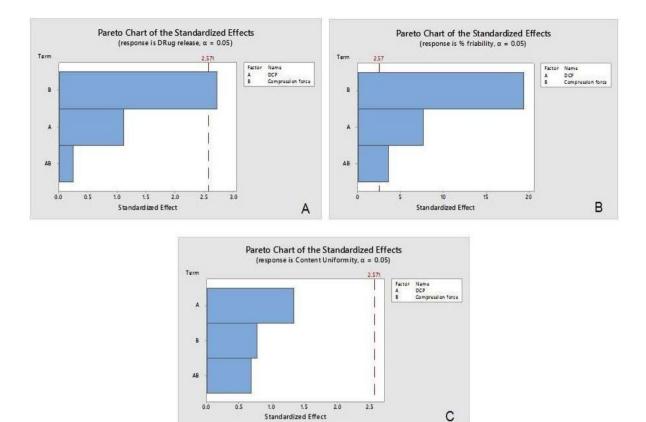
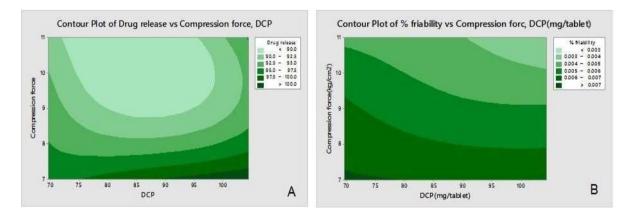


Figure No 4: Pareto Chart A) effect of DCP amount and compression force on Drug release B) effect of DCP amount and compression force on % friability C) effect of DCP amount and compression on Content uniformity.

Standardized Effect



Contour Plot of Content Uniformi vs Compression forc, DCP (mg/tablet)

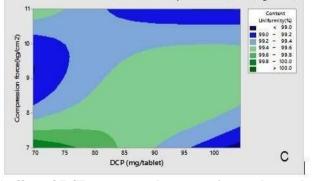


Figure No 5: Contour Plot A) effect of DCP amount and compression on drug release B) effect of DCP amount and compression on % friability C) effect of DCP amount and compression on content uniformity.

4. CONCLUSION

Formulation development encounters hundreds of problems due to process variables and thereby it's a time consuming process. Design of experiment helped formulation development department significantly in overcoming those problems and identifying the causes. This study helped in understanding the correlation between the variables and optimizing a robust formulation. The concept can be applied in developing other formulation.

5. COMPLIANCE WITH ETHICAL STANDARDS

This article does not contain any studies with human or animal subjects performed by any of the authors.

6. CONFLICT OF INTEREST

No conflict of interest associated with this work.

7. REFERENCES

- 1. Ali J, Ali N, Sultana Y, Baboota S, Faiyaz S. Development and validation of a stabilityindicating HPTLC method for analysis of antitubercular drugs. Acta Chromatographica, Jan 1, 2007; 18: 168.
- Huang J, Goolcharran C, Ghosh K. A Quality by Design approach to investigate tablet dissolution shift upon accelerated stability by multivariate methods. European Journal of Pharmaceutics and Biopharmaceutics, May 31, 2011; 78(1): 141-50.
- Sebhatu T, Ahlneck C, Alderborn G. The effect of moisture content on the compression and bondformation properties of amorphous lactose particles. International journal of pharmaceutics, Jan 1, 1997; 146(1): 101-14.
- 4. Rios M. Developments in powder flow testing. Pharmaceutical technology, 2006; 30(2).
- 5. Sorensen AH, Sonnergaard JM, Hovgaard L. Bulk characterization of pharmaceutical powders by low-pressure compression II: effect of method settings and particle size. Pharmaceutical development and technology, 2006; 11(2): 235-41.
- 6. Zhang Y, Law Y, Chakrabarti S. Physical properties and compact analysis of commonly used direct compression binders. aaps Pharmscitech, Dec 1, 2003; 4(4): 489-99.
- Gohel MC, Jogani PD. Functionality testing of a multifunctional directly compressible adjuvant containing lactose, polyvinylpyrrolidone, and croscarmellose sodium. Pharmaceutical technology, 2002; 26(3): 64-82.
- Li Q, Rudolph V, Weigl B, Earl A. Interparticle van der Waals force in powder flowability and compactibility. International journal of pharmaceutics, Aug 6, 2004; 280(1): 77-93.
- Lieberman HA, Rieger MM, Banker GS, editors. Pharmaceutical Dosage Forms-- Disperse Systems. M. Dekker, 1998.
- 10. Nystrom C, Alderborn G, Duberg M, Karehill PG. Bonding surface area and bonding mechanism-two important factors fir the

understanding of powder comparability. Drug development and industrial pharmacy, Jan 1, 1993; 19(17-18): 2143-96.

- 11. Luangtana-Anan M, Fell JT. Bonding mechanisms in tabletting. International journal of pharmaceutics, May 21, 1990; 60(3): 197-202.
- 12. Sonnergaard JM. Quantification of the compactibility of pharmaceutical powders. European Journal of Pharmaceutics and Biopharmaceutics. 2006 Jul 31;63(3):270-7.
- Cavazzuti M. Optimization methods: from theory to design scientific and technological aspects in mechanics. Springer Science & Business Media; 2012 Sep 11.
- 14. Bushra R, Shoaib MH, Aslam N, Hashmat D, Rehman M. Formulation development and optimization of ibuprofen tablets by direct compression method. Pak. J. Pharm. Sci. 2008 Apr 1; 21(2): 113-20.
- Dokala GK, Pallavi C. Direct compression-an overview. Int J Res Pharm Biomed Sci., Mar, 2013; 4(1): 155-8.
- 16. Furlanetto S, Cirri M, Maestrelli F, Corti G, Mura P. Study of formulation variables influencing the drug release rate from matrix tablets by experimental design. European journal of pharmaceutics and biopharmaceutics, Jan 31, 2006; 62(1): 77-84.
- Ford JL. Design and evaluation of hydroxypropyl methylcellulose matrix tablets for oral controlled release: A historical perspective. InHydrophilic Matrix Tablets for Oral Controlled Release, 2014; 17-51. Springer New York.
- 18. Golden MP, Vikram HR. Extrapulmonary tuberculosis: an overview. American family physician, Nov 1, 2005; 72(9).
- 19. Fernandez EG, Cordero S, Benítez M, Perdomo I, Morón Y, Morales AE, Arce MG, Cuesta E, Lugones J, Fernández M, Gil A. Rapid development and optimization of tablet manufacturing using statistical tools. AAPS Pharm Sci Tech., Jun 1, 2008; 9(2): 620-7.
- 20. Hiremath PS, Saha RN. Controlled release hydrophilic matrix tablet formulations of isoniazid: design and in vitro studies. Aaps Pharmscitech, Dec 1, 2008; 9(4): 1171-8.
- 21. Gohel MC, Jogani PD. A review of co-processed directly compressible excipients. J Pharm Pharm Sci, Apr 16, 2005; 8(1): 76-93.
- 22. Gohel MC, Parikh RK, Padshala MN, Sarvaiya KG, Jena DG. Formulation and optimization of directly compressible isoniazid modified release matrix tablet. Indian Journal of Pharmaceutical Sciences, 2007; 69(5): 640.
- 23. Ulla SN, Roy AK, SM VK. Formulation and evaluation of sustained release matrix tablets of lornoxicam. International Journal of Drug Development and Research, 2011; 3(1).
- 24. Minitab Inc (2016), Getting started with minitab.

- https://www.minitab.com/uploadedFiles/Documents/ getting-started/Minitab17_GettingStarted-en.pdf accessed on 14 July 2015
- 26. Indian Pharmacopoeia, Government of India Ministry of Health & Family Welfare Published by the Indian Pharmacopoeia Commission, Ghaziabad, 2007; 323-24.
- Campisi B, Chicco D, Vojnovic D, Phan-Tan-Luu R. Experimental design for a pharmaceutical formulation: optimisation and robustness. Journal of pharmaceutical and biomedical analysis, Oct 31, 1998; 18(1): 57-65.
- Kumar DA, Kumar PK, Ranjita D, Murthy PN, Kumar A. Method development, validation and stability study of repaglinide in bulk and pharmaceutical dosage form by UV spectrometric method. Int. J. Biol. & Pharm. Res., 2011; 2: 7-10.
- 29. US Pharmacopoeia 30/NF25, Chapter 711: dissolution. US Pharmacopoeial Convention, Rockville, 2007.
- Levina M, Rajabi-Siahboomi AR. The influence of excipients on drug release fromhydroxypropyl methylcellulose matrices. Journal of pharmaceutical sciences, Nov 1, 2004; 93(11): 2746-54.
- 31. Huang Y, Khanvilkar KH, Moore AD, Hilliard-Lott M. Effects of manufacturing process variables on in vitro dissolution characteristics of extended-release tablets formulated with hydroxypropyl methylcellulose. Drug development and industrial pharmacy, Jan 1, 2003; 29(1): 79-88.
- 32. Szymczak MM, Friedman RL, Uppoor R, Yacobi A. Detection, measurement, and control in pharma manufacturing. Pharm Technol, 2011; 35: 70-6.